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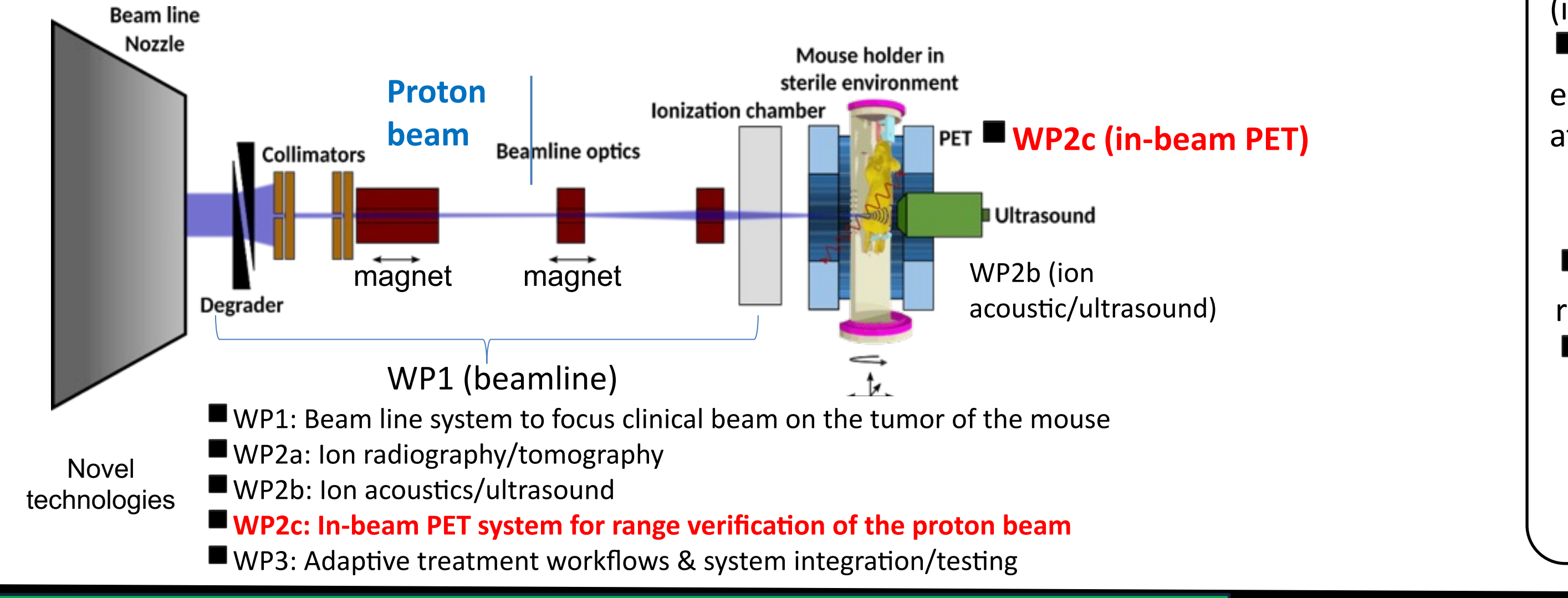
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## 1. Introduction: SIRMIO project and high-resolution Small Animal in-beam PET system

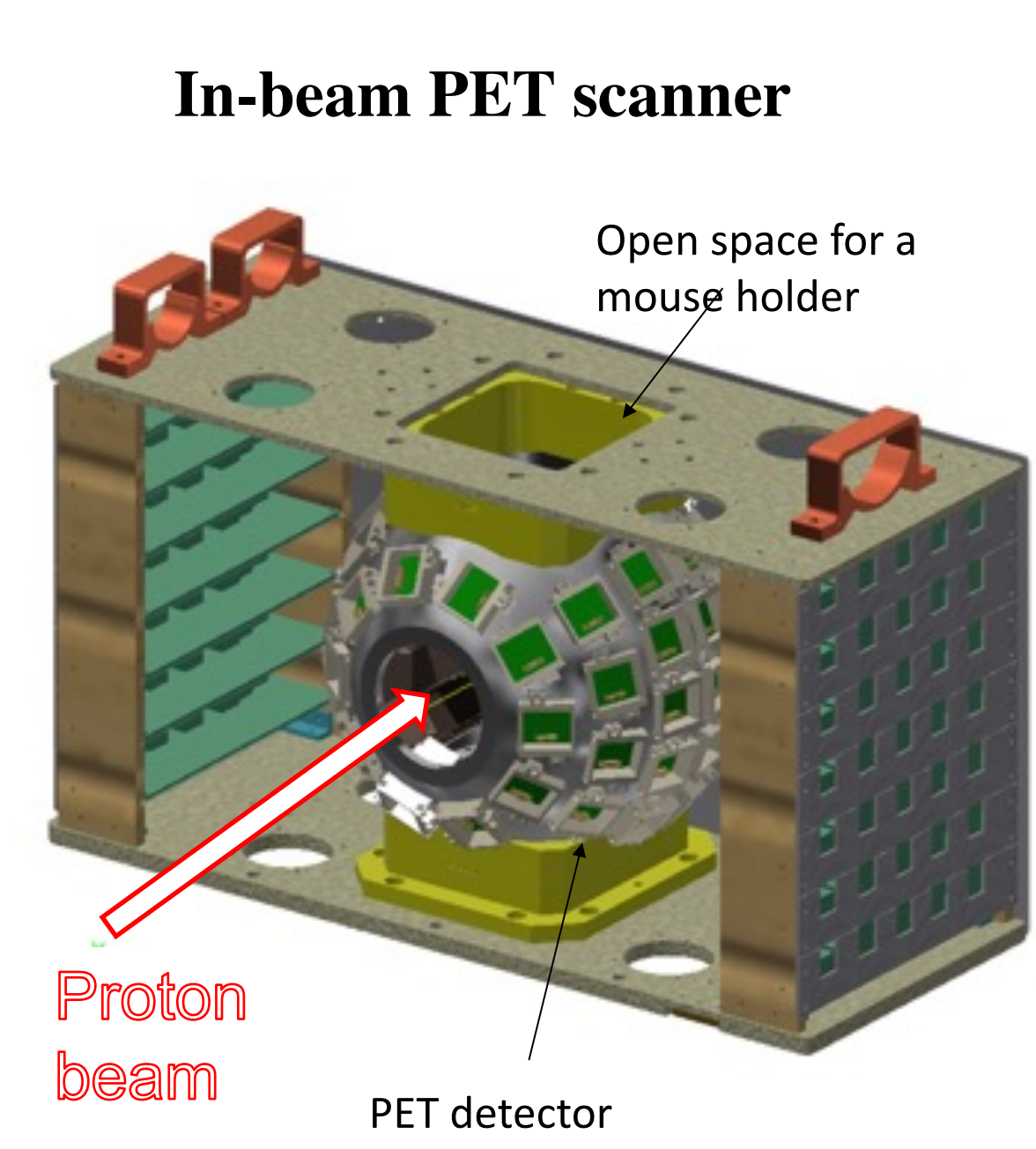
### Small animal proton Irradiator for Research in Molecular Image-guided radiation-Oncology: SIRMIO project [1] (www.lmu.de/sirmio)

The purpose of the SIRMIO project is to build a portable beam-line equipped with novel detector technologies for integration in clinical facilities. In-beam PET is used to image positron emitter distributions generated by interaction between the target and the proton beam



### Requirement and design

- Open space for beam directors, mouse holder and additional detectors (ionacoustic/US)
- High sensitivity for a few kBq positron emitters generated by the proton beam at typical treatment dose levels
- Spherical shape
- Sub-millimeter image resolution for range monitoring in small animal
- Uniform spatial image resolution
- High resolution depth of interaction (DOI) PET detector



### In this poster

- Introduction of the High-resolution DOI PET detector developed by us
- Two imaging performance studies:
  - Imaging of point sources with the PET scanner designed for the SIRMIO project
  - Capability of our high-resolution PET detector for imaging of radioactive ion beams with in-beam PET system

## 2. Sub-millimeter resolution PET Detector

### 2-1 Detector components (collaboration with QST) [2]

**Scintillator block**

- Pixel size: 0.9 mm x 0.9 mm x 6.67 mm
- 3 layer structure
- 1st layer: 20 x 23 crystals
- 2nd layer: 23 x 23 crystals
- 3rd layer: 24 x 24 crystals
- Reflector between scintillator pixels : BaSO<sub>4</sub>

**Photo detector (SiPM)**

- Multi Pixel Photon Counter (MPPC, Hamamatsu photonics K.K, S14161-3050HS-08, Japan)
- Array: 8 x 8 (64 signals)
- Active area: 3 mm x 3 mm
- Dimension: 25.8 mm x 25.8 mm
- Optical coupling with RTV rubber (SE-420, shin-etsu, Japan)

**Readout circuit board**

(a) Charge division circuit (CDC)

(b) Amplifier circuit

**Digitizer R5560 (CAEN, Italy)**

Input: Analog (differential signal ethernet cable, RJ45)

# of channel: 128 channels (32 detectors)

sampling frequency: 125 MHz (default mode)

- FPGA is configurable to user's purpose
- Can operate as oscilloscope and in QDC mode
- External trigger is acceptable and can output logic signal.
- C++ libraries for data acquisition are provided by CAEN.
- Scalable with other CAEN digitizers.

### 2-2 Anger calculation

**3-layer staggered array**

**Flood map**

Anger calculation

$$x = \frac{(s_2 + s_4) - (s_1 + s_3)}{\sum s_i}$$

$$y = \frac{(s_1 + s_2) - (s_3 + s_4)}{\sum s_i}$$

Crystal response

- 1st layer
- 2nd layer
- 3rd layer

Each crystal response corresponds to scintillator pixel. 3D information of the interaction is projected on the 2D histogram

### 2-3 detector response (Na-22 source)

**Light output**

**Flood map**

**Zoomed flood map**

Crystal responses are clearly separated at the center

**0.9 mm pixel resolution & 6.67 mm depth resolution**

## 3. Imaging Experiment with the high-resolution PET detector

Image was reconstructed with the MEGALib software which is Geant4 based simulation and reconstruction toolkit originally developed for Compton cameras [3]. Reconstruction of PET image has been implemented.

### 3-1 SIRMIO PET scanner (point source measurement)

**The SIRMIO PET scanner**

**Geometry**

- Inner radius: 72 mm
- Number of detectors: 56
- Number of rings: 6
- coverage: 44%

Open space for a mouse holder

PET detector

Birdcage housing

Beam

**Na-22 source setup**

A Na-22 point source with a diameter of 1 mm was placed 2 mm pitch along Z with a moving stage and measured for 2 minutes. Data of each point was merged and used for reconstruction.

Gap: 1 mm

Diameter: 1 mm

Na-22 (140 kBq)

Pitch: 2 mm

**Imaging result**

Reconstructed image

11356 events

1 mm

**Line profile**

Voxel value [a.u.]

Z [mm]

**Outlook**

- 1 mm imaging resolution is achieved.

### 3-2 Radioactive Carbon Ion Beam Imaging

"Biomedical Application of Radioactive Beams" (BARB) project at GSI Darmstadt [4] (www.gsi.de/BARB)

Goal of the BARB project is to exploit GSI's capability of generating radioactive ion (RI) beams to demonstrate their image guidance advances in small animal studies with a novel imaging system.

**setting**

GSI beam line

Cross shape arrangement

PET detector

3D printed support

**Geometry and target**

Phantom: PMMA (25 cm x 12 cm x 35 cm)

Phantom position was set so that Bragg peak was at the center of the PET FOV

C-11 beam

PET detector

phantom

PET Measurement time: 60 min

Beam on 40 min & beam off 20 min

**Beam properties**

Ion: C-11, Intensity: ~10<sup>7</sup> particles/s

- Achromatic beam
- Energy: 256 MeV/u
- Momentum spread: 11.8 MeV/c/u
- Width of 80% dose: 3.92 mm

- Monochromatic beam
- Energy: 257 MeV/u
- Momentum spread: 2 MeV/c/u
- Width of 80% dose: 1.54 mm
- Narrower peak

Depth dose distributions of achromatic and monochromatic beams of C-11 in water

**Imaging result**

Achromatic

Monochromatic

Voxel size: 0.5 mm x 0.5 mm x 0.5 mm

Field of view: 2.4 cm(X) x 2.4 cm(Y) x 4.8 cm(Z)

Method: MLEM

Iteration: 8

Geometrical sensitivity correction

**Line profiles**

Standard deviation

Achr.: 2.0 mm

Mon.: 1.1 mm

**Outlook**

- high resolution PET detector helps to resolve small difference of the RI beam distribution.

## 4. Conclusion & future work

- The SIRMIO PET scanner shows 1 mm image resolution.
- Our PET detector is useful for imaging the RI beam and resolving a few mm distribution difference.
- An experiment for imaging proton beams with the SIRMIO is planned in September 2022.
- Simulation study of the RI beams is ongoing for the BARB project in preparation of small animal experiments.

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**References :**

[1] K. Parodi, et al. Towards a novel small animal proton irradiation platform: the SIRMIO project; *Acta Oncologica*; (2019), 58, 1470-1475, [2] 2021, Kang et al., *BPEX*, vol 7, no. 3, pp. 035018, [3] G. Lovatti et al., 2020 IEEE NSS/MIC, M-08-275, [4] Durante M and Parodi K (2020) *Radioactive Beams in Particle Therapy: Past, Present, and Future*. *Front. Phys.* 8:326.