

Challenges in the Boron Neutron Capture Therapy



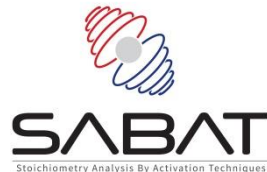
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- ❖ Introduction
- ❖ Neutron sources for BNCT
- ❖ Boron carriers
- ❖ Dose and boron distribution monitoring
- ❖ Gadolinium Neutron Capture Therapy
- ❖ Summary



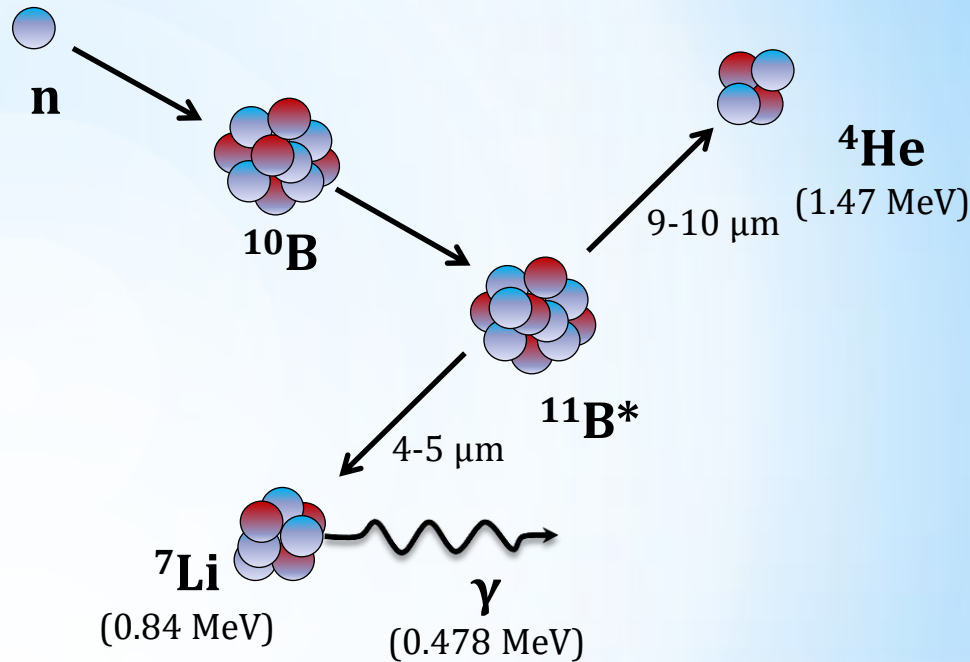
Narodowe Centrum
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Introduction

- ❖ Therapy used against highly malignant and therapeutically resistant tumors:
 - ❖ glioblastoma multiforme)
 - ❖ malignant melanoma
 - ❖ head and neck recurrent cancers
 - ❖ Malignant pleural mesothelioma
- ❖ Irradiation with (epi)thermal neutrons
- ❖ ^{10}B transferred selectively to the tumor cells
- ❖ High LET within a single cell



Introduction

- ❖ So far only ^{10}B and Gd were considered as „targets” for NCT

$$D_{\text{tot}} = CBE_B D_B + 3.2D_n + 3.2D_H + D_\gamma$$

$^{10}\text{B}(n,\alpha)^7\text{Li}$ $^{14}\text{N}(n,p)^{14}\text{C}$ p recoil $^1\text{H}(n,\gamma)^2\text{H}$

Compound Biological Effectiveness Relative Biological Effectiveness

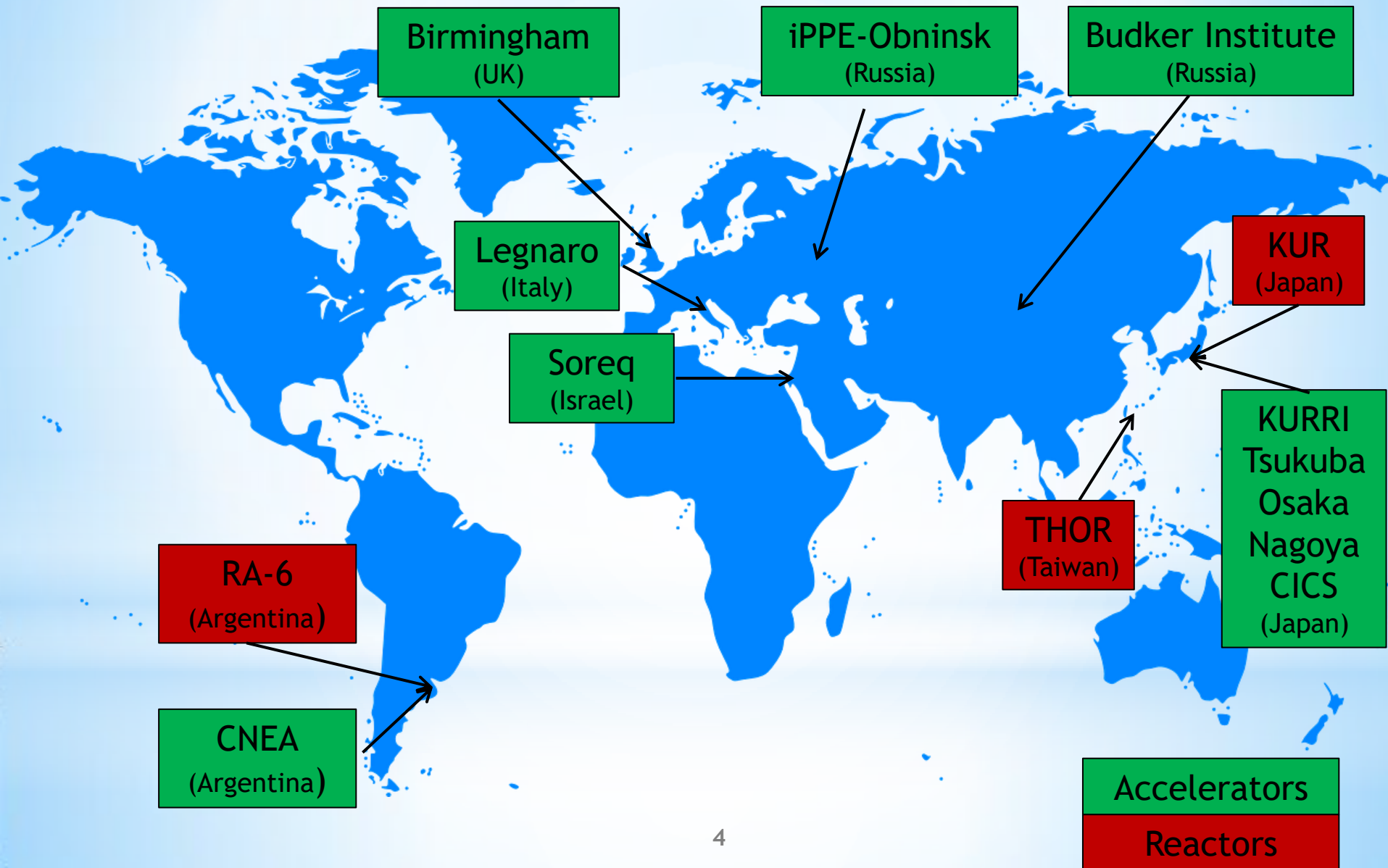
- ❖ The in-air neutron beam recommendations by the International Atomic Energy Agency:

Parameter	Recommendations
$\Phi_{\text{epi}} (0.1 \text{ eV} < E_n < 10 \text{ keV}) [\text{cm}^{-2}\text{s}^{-1}]$	$> 10^9$
$\Phi_{\text{epi}} / \Phi_{\text{thermal}}$	> 20
$\Phi_{\text{epi}} / \Phi_{\text{fast}}$	> 100
$D_{\text{fast}} / \Phi_{\text{epi}} [\text{Gy cm}^2]$	$< 2 \cdot 10^{-13}$
$D_\gamma / \Phi_{\text{epi}} [\text{Gy cm}^2]$	$< 2 \cdot 10^{-13}$

Nuclide	Reaction	σ [b]
^3He	(n,p)	5333
^6Li	(n, α)	940
^{10}B	(n,α)	9835
^{113}Cd	(n, γ)	20600
^{135}Xe	(n, γ)	2720000
^{149}Sm	(n, γ)	42080
^{151}Eu	(n, γ)	9200
^{155}Gd	(n,γ)	61100
^{157}Gd	(n,γ)	259000
^{147}Hf	(n, γ)	561
^{199}Hg	(n, γ)	2150

(Wolfgang A.G. Sauerwein, A. Wittig, R. Moss, Y. Nakagawa „Neutron capture therapy”, Springer)

BNCT facilities around the world (2016)



Neutron sources for BNCT

❖ Reactors

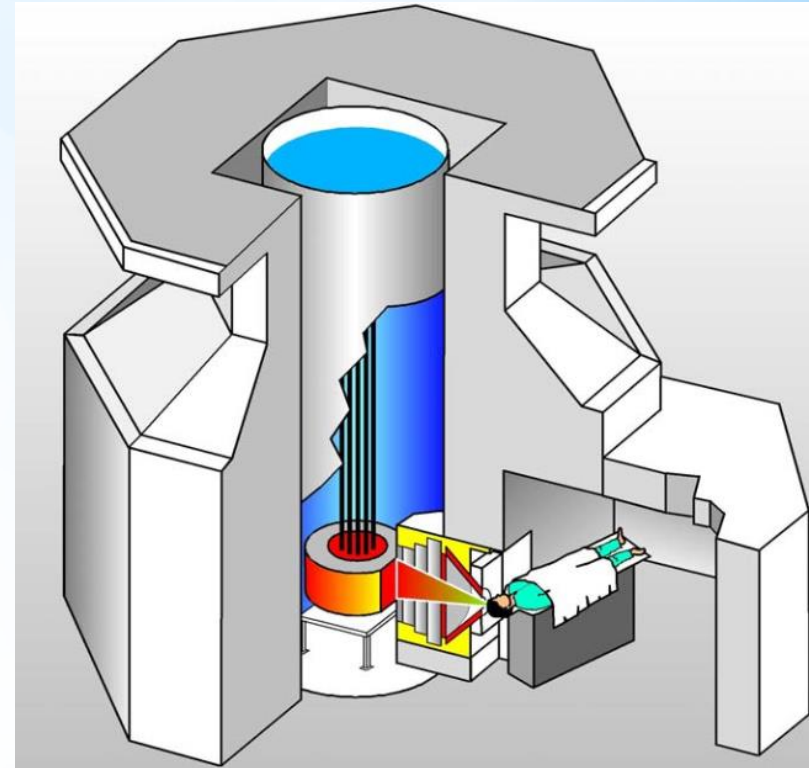
- ❖ High neutron flux (e.g. Maria: $\sim 10^{14}$ cm⁻²s)
- ❖ Expensive and complex
- ❖ low public acceptability
- ❖ require complicated licensing procedures

Reactor BNCT beams



core neutrons
(fast→epithermal)

fission converter
(thermal→epithermal)



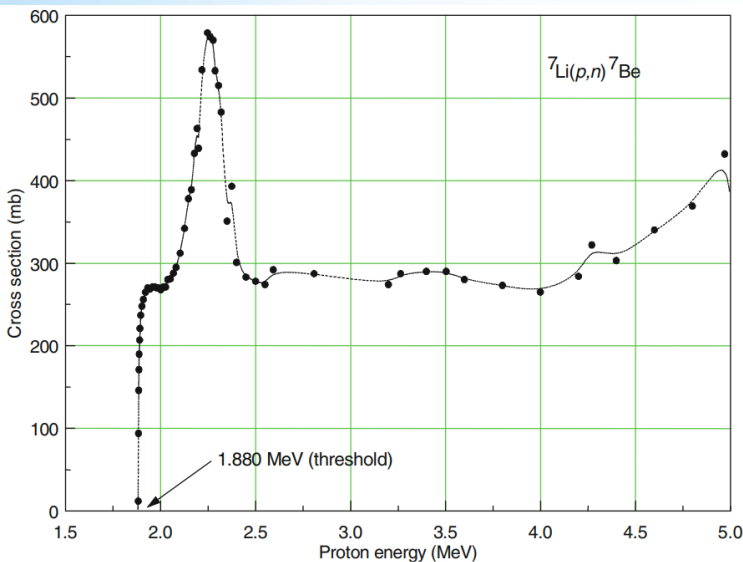
❖ Isotopic sources (e.g. Sb-Be, Am-Be)

- ❖ High activities needed (orders of magnitude higher than therapeutic gamma sources)
- ❖ Cannot be switched off
- ❖ Never used, simulations showed feasibility of such therapy [M. Golshanian et al., Nucl. Inst. Meth. A 835 (2016) 182]

Neutron sources for BNCT

❖ Accelerator sources

- ❖ Expensive
- ❖ Require a lot of space
- ❖ Most popular reactions: ${}^7\text{Li}(p,n){}^7\text{Be}$ and ${}^9\text{Be}(p,n){}^9\text{B}$
- ❖ Target cooling problems for high proton intensity

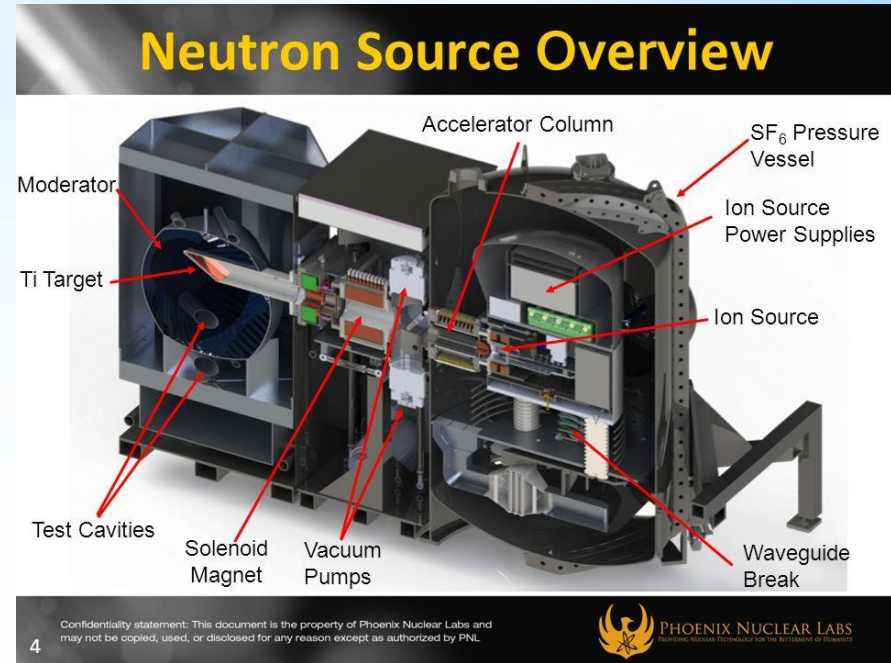


Reaction	E_{th} (MeV)	E_{in} (MeV)	Total production (n/mA s)	Fraction $E_n < 1$ MeV (%)	$E_{n,max}$ (keV)	$E_{n,min}$ (keV)
${}^7\text{Li}(p,n){}^7\text{Be}$	1.880	1.880	0	100	30	30
		1.890	6.3×10^9	100	67	0.2
		2.500	9.3×10^{11a}	100	787	60
		2.800	1.4×10^{12b}	92	1,100	395
${}^9\text{Be}(p,n){}^9\text{B}$	2.057	2.057	0	100	20	20
		2.500	3.9×10^{10}	100	574	193
${}^9\text{Be}(d,n){}^{10}\text{B}$	0	0	0	50	3,962	3,962
		1.500	3.3×10^{11}	50	4,279	3,874
${}^{13}\text{C}(d,n){}^{14}\text{N}$	0	0	0	75	4,974	4,964
		1.500	1.9×10^{11}	70	6,772	5,616
${}^{12}\text{C}(d,n){}^{13}\text{N}$	0.327	0.327	0	100	4	3
		1.500	6.0×10^{10}	80	1,188	707
$d(d,n){}^3\text{He}$	0	0	0	0	2,451	2,451
		0.120	3.3×10^{8c}	0	2,898	2,123
		0.200	1.1×10^9	0	3,054	2,047
$t(d,n){}^4\text{He}$	0	0	0	0	14,050	14,050
		0.150	4.5×10^{10}	0	14,961	13,305

(Wolfgang A.G. Sauerwein, A. Wittig, R. Moss, Y. Nakagawa „Neutron capture therapy”, Springer)

Neutron sources for BNCT

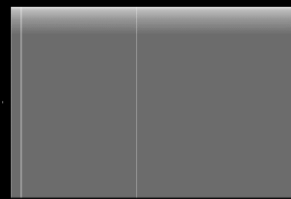
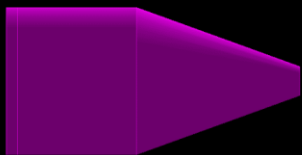
- ❖ Neutron generators: DD or DT
 - ❖ Small size and cost
 - ❖ Fast, monochromatic neutrons
 - ❖ Max. intensities $\sim 10^{11}/s$ (DD) - 10^{13} (DT) [Phoenix]
 - ❖ Never used so far (too low neutron intensities)
- ❖ Each of the source need a Beam Shaping Assembly to form the desired epithermal neutron beam



1. Moderators

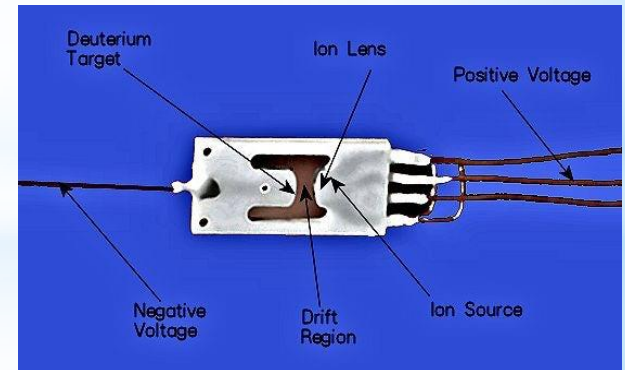


2. Lead Reflector



3. Concrete Shielding

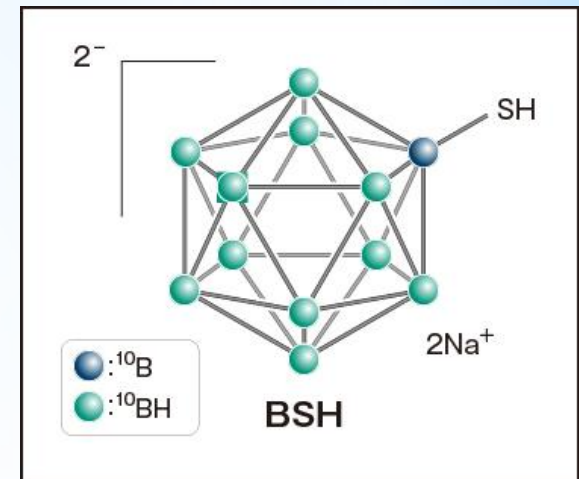
Courtesy of Vahagn Ivanyan



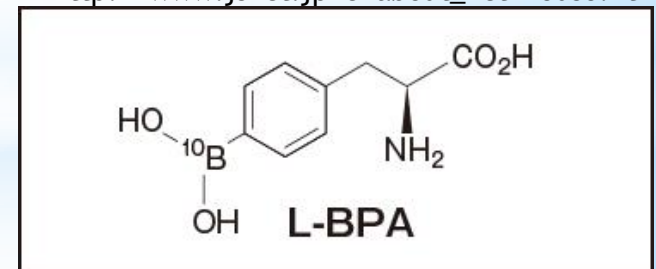
<https://newatlas.com/sandia-neutristor-neutron-generator-chip/23856/#gallery>

Boron carriers

- ❖ Selective accumulation (Tumor/Normal >3) with ^{10}B concentration of 20 to 40 ppm
 - ❖ Low toxicity
 - ❖ Not metabolized in the tumor
 - ❖ No pharmaceutical effects themselves (boron delivery molecule only)
-
- ❖ BSH (disodium mercaptoundecahydrododecaborate)
 - ❖ Low accumulation inside tumor cells (it stays in the intercellular spaces)
 - ❖ L-BPA (L-p-Boronophenylalanine)
 - ❖ Administered combined with a water-soluble substance such as D-fructose
 - ❖ does not accumulate in slowly proliferating malignant cells

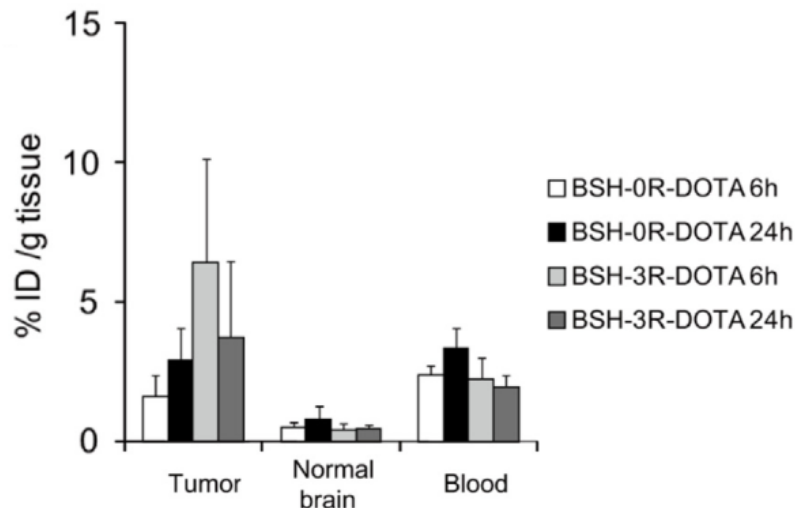
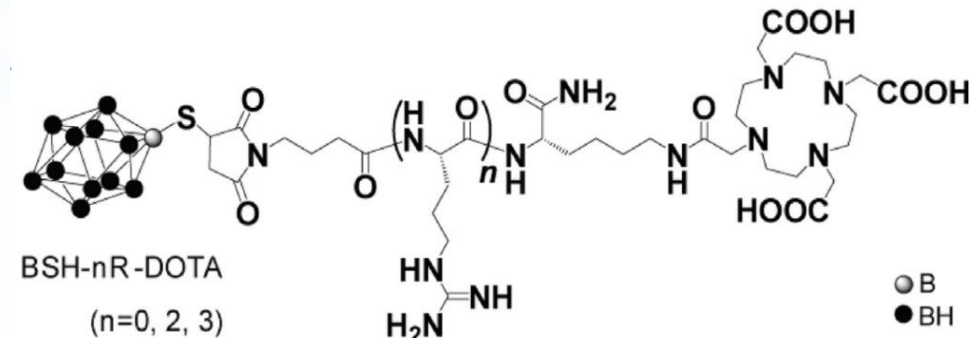


http://www.jsnct.jp/e/about_nct/houso.html

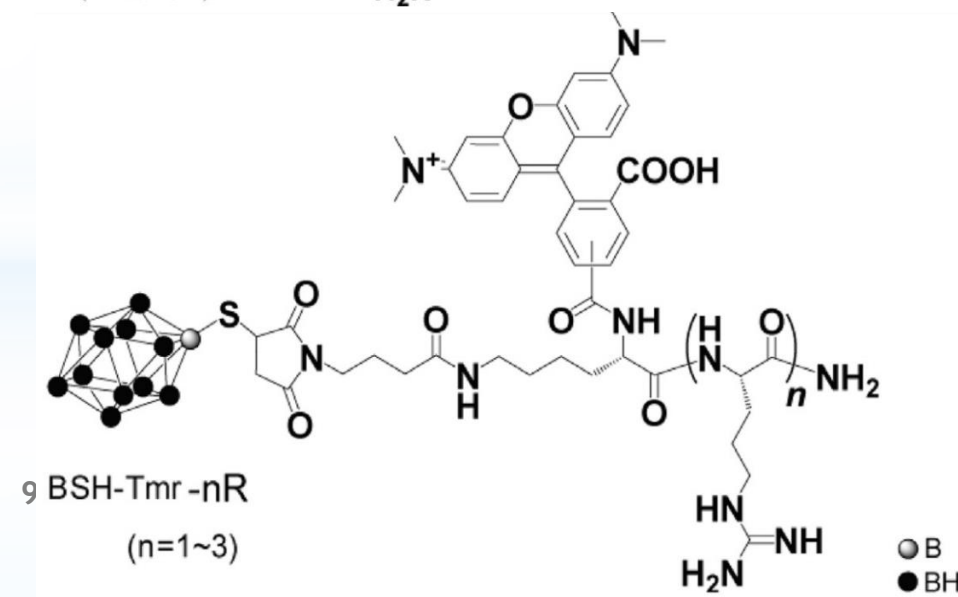


Boron carriers

- ❖ Intensive studies are ongoing to increase the tumor selectivity and intracellular delivery of ^{10}B -compounds
 - ❖ BSH connected to e.g. protein, peptide, small-interfering RNA...
 - ❖ Carborane-bearing pullulan nanogels [R. Kawasaki et al., Biochemical and Biophysical Research Communications 483 (2017) 147]
 - ❖ BSH-polymer conjugates, e.g. PEG-b-P(Glu-SS-BSH) [P. Mi et al., Journal of Controlled Release 254 (2017) 1]



(Iguchi Y. et al. Biomaterials 56 (2015) 10-17)



Dose and boron distribution monitoring

❖ Magnetic Resonance Imaging (MRI)

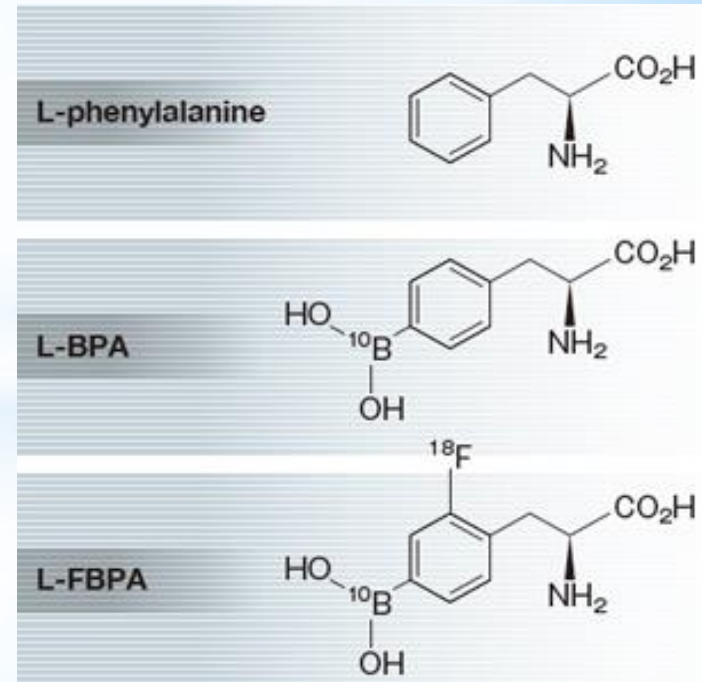
- Non-invasive imaging of boron distribution
- Sensitive to ^{10}B and ^{11}B isotopes

❖ Activation Gamma Radiation Analysis

- Gamma quanta due to neutron capture on ^{10}B ($E_\gamma = 0.478 \text{ MeV}$)
- Radiation of tissue activation (H,C,N,...)
- A fast method that allows in vivo imaging also during therapy

❖ Positron Emission Tomography

- Boron carrier labeled with β^+ active element:
- L-F-Boronophenylalanine [Imahori Y. et al. J Nucl Med. 39 (1998) 325]
- ^{64}Cu -labeled BSH-3R-DOTA [Y. Iguchi et al., Biomaterials 56 (2015) 10]
- Non-invasive imaging of boron distribution in the patient's body at each stage of therapy (resolution ~ 4-6 mm)



Alternatives to Boron

- ❖ $^{157}\text{Gd}(n,\gamma)^{158}\text{Gd}$ reaction has 60 times bigger cross section than the capture on ^{10}B
- ❖ Easy assessment of the Gd concentration in the tissue to be used in the treatment by MRI

GdNCT = short range contribution (Auger electrons) + long range products (gammas)

- ❖ **Efficient therapy demands Gd transfer to the cell nucleus**
[S. A. Enger et al., Radiation Measurements 59 (2013) 233]

Summary

physicsworld

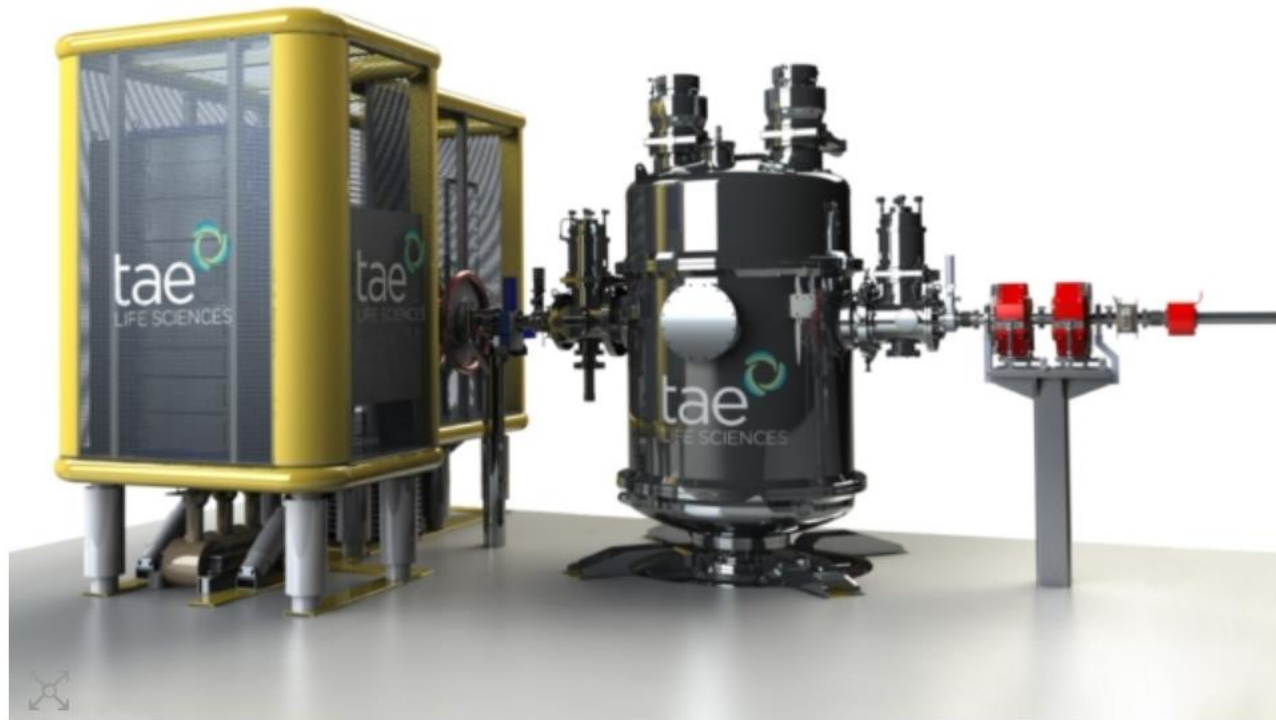


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RADIOTHERAPY | RESEARCH UPDATE

Boron neutron capture therapy progresses towards clinical cancer treatments

17 May 2019 [Tami Freeman](#)



***BACKUP**

